Introduction to Computational Neuroscience

Biol 698 Math 635 Biol 498 Math 430

Bibliography:

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- The passive membrane equation (review)
- Goldman-Hodgkin-Katz equation
- Mechanism of action potential generation
- Hodgkin-Huxley equation

Nernst equation (review)



Figure 2.2: Diffusion of K^+ ions down the concentration gradient though the membrane (a) creates an electric potential force pointing in the opposite direction (b) until the diffusion and electrical forces counter each other (c). The resulting transmembrane potential (2.1) is referred to as the Nernst equilibrium potential for K^+ .

Nernst equation (review)

The membrane potential is at rest when the net crossmembrane current is equal to zero

✓ Nernst Equation:

$$\Xi_{X} = \frac{R T}{z F} \ln \frac{C_{X,out}}{C_{X,in}}$$

- E_X: Equilibrium potential of ion X
- R: gas constant (1.98 cal/°K-mol)
- F: Faraday's constant (96,480 C/mol))
- z: Valence
- T: Temperature (°K)

Nernst equation (review)

✓ Reversal potentials:

Table 1.1 Typical ion concentrations in cells (from Johnston and Wu [139])			
Ion	Inside (mM)	Outside (mM)	Equilibrium potential (mV), $E_i = \frac{RT}{zF} \ln \frac{[C]_{out}}{[C]_{in}}$
Frog muscle			$T = 20^{\circ}C$
K ⁺	124	2.25	$58 \log \frac{2.25}{124} = -101$
Na ⁺	10.4	109	$58 \log \frac{109}{10.4} = +59$
CI ⁻	1.5	77.5	$-58 \log \frac{77.5}{1.5} = -99$
Ca ²⁺	10 ⁻⁴	2.1	$29\log\frac{2.1}{10^{-4}} = +125$
Squid axon			$T = 20^{\circ}C$
K+	400	20	$58 \log \frac{20}{400} = -75$
Na ⁺	50	440	$58 \log \frac{440}{50} = +55$
Cl-	40-150	560	$-58 \log \frac{560}{40-150} = -66 \text{ to } -33$
Ca ²⁺	10 ⁻⁴	10	$29\log \frac{10}{10^{-4}} = +145$
Mammalian cell			$T = 37^{\circ}C$
К+	140	5	$62 \log \frac{5}{140} = -89.7$
Na ⁺	5–15	145	$62\log\frac{145}{5-15} = +90 - (+61)$
Cl-	4	110	$-62\log\frac{110}{4} = -89$
Ca ²⁺	10 ⁻⁴	2.5–5	$31\log\frac{2.5-5}{10^{-4}} = +136 - (+145)$

Equivalent circuit model (review)

Components

• Capacitors: representing the ability of the membrane to store charge

• batteries: representing the concentration gradients of the ions

conductors or resistors: representing the ion channels



membrane only permeable to K⁺

Fig. 1.2 The cell membrane showing the insulating lipid bilayer and a K⁺ channel, which allows current to flow. The equivalent electrical circuit is shown on the *right*

Passive membrane equation (review)

Intrinsic electric circuit + Injected (Iinj) or applied current (Iapp)

Kirchhoff's current law:

The total current into the cell must add up to z



$$C\frac{dV}{dt} = -G_{L}(V-E_{L}) + I_{inj}(t)$$

$$C\frac{dV}{dt} = -G_{L}(V-E_{L}) + I_{app}(t)$$

Passive membrane equation

time constant:

 $\tau = R C$

$$C\frac{dV}{dt} = -G_{L}(V-E_{L}) + I_{inj}(t)$$

 $\tau \frac{dV}{dt} = -V + E_L + I_{inj}(t)R$

Passive membrane equation (review)

• $I_{app} = I_0$ (const) $V_{\infty} = R I_0$

$$V(t) = \left[V_{\infty} + E_{L} \right] + \left(V_{0} - E_{L} - V_{\infty} \right) e^{-t/\tau}$$

steady state

• $V_0 = E_L$

$$V(t) = \left[V_{\infty} + E_{L} \right] - V_{\infty} e^{-t/\tau}$$

steady state



Goldman-Hodgkin-Katz equation:

$$E_{m} = \frac{R T}{F} \ln \frac{P_{K^{+}}[K^{+}]_{o} + P_{Na^{+}}[Na^{+}]_{o} + P_{Cl^{-}}[Cl^{-}]_{i}}{P_{K^{+}}[K^{+}]_{i} + P_{Na^{+}}[Na^{+}]_{i} + P_{Cl^{-}}[Cl^{-}]_{o}}$$

P_X: Permeability of ion X

R, T, F: Gas constant, Temperature (°K) and Faraday constant

Goldman-Hodgkin-Katz equation:

$$E_{m} = \frac{R T}{F} \ln \frac{[K^{+}]_{o} + b [Na^{+}]_{o}}{[K^{+}]_{i} + b [Na^{+}]_{i}} \qquad b = \frac{P_{Na}}{P_{K^{+}}}$$

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$$E_{m} = \frac{R T}{F} \ln \frac{[K^{+}]_{o} + b [Na^{+}]_{o}}{[K^{+}]_{i} + b [Na^{+}]_{i}} \qquad b = \frac{P_{Na^{+}}}{P_{K^{+}}}$$

$$[Na^{+}]_{o} = 145 \frac{\text{mmol}}{L} [Na^{+}]_{i} = 10 \frac{\text{mmol}}{L} E_{Na^{+}} = +67 \text{ mV}$$
$$[K^{+}]_{o} = 5 \frac{\text{mmol}}{L} [K^{+}]_{i} = 140 \frac{\text{mmol}}{L} E_{Na^{+}} = -84 \text{ mV}$$

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Membrane 20 times more permeable to K⁺ than to Na⁺:

b = 0.05 $E_m = -78 mV$

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Membrane 10 times more permeable to Na⁺ than to K⁺:

b = 10 $E_m = +51 mV$

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$$E_{m} = \frac{R T}{F} \ln \frac{[K^{+}]_{o} + b [Na^{+}]_{o}}{[K^{+}]_{i} + b [Na^{+}]_{i}} \qquad b = \frac{P_{Na^{+}}}{P_{K^{+}}}$$

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Membrane 5 times more permeable to K⁺ than to Na⁺:

b = 0.2 $E_m = -61 mV$



Fig. 1.7 The action potential. During the upstroke, Na^+ channels open and the membrane potential approaches the Na^+ Nernst potential. During the downstroke, Na^+ channels are closed, K^+ channels are open, and the membrane potential approaches the K^+ Nernst potential

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Membrane 20 times more permeable to K⁺ than to Na⁺:

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Hodgkin & Huxley (1949) demonstrated that:

- The resting membrane of a squid axon is 25 times more permeable to K+ than to Na+
- At the peak of an action potential the membrane is 20 times more permeable to Na⁺ than to K⁺.
- During after hyperpolarization the membrane permeability to Na+ is very low and that of K+ is larger than at rest

✓ Major ionic currents:

$$I_{\rm K} = g_{\rm K} \left(V - E_{\rm K} \right) \qquad I_{\rm Na} = g_{\rm Na} \left(V - E_{\rm Na} \right) \qquad I_{\rm Ca} = g_{\rm Ca} \left(V - E_{\rm Ca} \right) \qquad I_{\rm Cl} = g_{\rm Cl} \left(V - E_{\rm Cl} \right)$$



Figure 2.3: Equivalent circuit representation of a patch of cell membrane.

Kirchhoff's current law: the total current flowing across a patch of cell membrane is the sum of the membrane capacitive current and all the ionic currents.





$$CV = I - I_{\rm Na} - I_{\rm Ca} - I_{\rm K} - I_{\rm Cl}$$

 $C\dot{V} = I - g_{\text{Na}}(V - E_{\text{Na}}) - g_{\text{Ca}}(V - E_{\text{Ca}}) - g_{\text{K}}(V - E_{\text{K}}) - g_{\text{Cl}}(V - E_{\text{Cl}})$

✓ Major ionic currents:

$$I_{\rm K} = g_{\rm K} \left(V - E_{\rm K} \right)$$

$$I_{\rm Na} = g_{\rm Na} \left(V - E_{\rm Na} \right)$$



$$C \frac{\mathrm{d}V}{\mathrm{d}t} = I -g_{\mathrm{Na}}(V - E_{\mathrm{Na}}) - g_{\mathrm{K}}(V - E_{\mathrm{K}}) - g_{\mathrm{L}}(V - E_{\mathrm{L}})$$



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 $C\dot{V} = I - g_{\text{Na}}(V - E_{\text{Na}}) - g_{\text{Ca}}(V - E_{\text{Ca}}) - g_{\text{K}}(V - E_{\text{K}}) - g_{\text{Cl}}(V - E_{\text{Cl}})$

$$C\dot{V} = I - g_{\rm inp}(V - V_{\rm rest})$$

 $g_{\rm inp} = g_{\rm Na} + g_{\rm Ca} + g_{\rm K} + g_{\rm Cl}$

$$V_{\text{rest}} = \frac{g_{\text{Na}}E_{\text{Na}} + g_{\text{Ca}}E_{\text{Ca}} + g_{\text{K}}E_{\text{K}} + g_{\text{Cl}}E_{\text{Cl}}}{g_{\text{Na}} + g_{\text{Ca}} + g_{\text{K}} + g_{\text{Cl}}}$$

$$C\dot{V} = I - g_{Na} (V - E_{Na}) - g_{Ca} (V - E_{Ca}) - g_{K} (V - E_{K}) - g_{Cl} (V - E_{Cl})$$

$$C\dot{V} = I - g_{\rm inp}(V - V_{\rm rest})$$

$$V_{\rm rest} = \frac{g_{\rm Na}E_{\rm Na} + g_{\rm Ca}E_{\rm Ca} + g_{\rm K}E_{\rm K} + g_{\rm Cl}E_{\rm Cl}}{g_{\rm Na} + g_{\rm Ca} + g_{\rm K} + g_{\rm Cl}}$$

 $g_{\rm inp} = g_{\rm Na} + g_{\rm Ca} + g_{\rm K} + g_{\rm Cl}$

input conductance

 $R_{inp} = 1/g_{inp}$ input resistance measures the asymptotic sensitivity of the membrane potential to injected (applied) or intrinsic currents

$$V \rightarrow V_{\text{rest}} + IR_{\text{inp}}$$



Figure 2.4: Mechanistic interpretation of the resting membrane potential (2.4) as the center of mass. Na⁺ conductance increases during the action potential.

Ionic channels:

- Transitions between open and closed states in individual channels are stochastic
- However, the net current I generated by a large population or ensemble of identical channels can be reasonably be described by

$$I = G_X p (V - E_X)$$

- p: average proportion of channels in the open state -----
- G_X: maximal conductance of the population
- E_X: reversal potential of the current (potential at which the current reverses its direction)

If the channels are selective for a single ionic species

reversal potential = Nernst potential for that ionic species

Ionic channels:



Figure 2.8: Structure of voltage-gated ion channels. Voltage sensors open activation gate and allow selected ions to flow through the channel according to their electrochemical gradients. The inactivation gate blocks the channel (modified from Armstrong and Hille 1998).

Voltage-gated ionic channels:

- Activating gates: open the channels
- Inactivating gates: close the channels

 $I = G_X p (V - E_X)$

 $p = m^a h^b$

- m = 1: activated
- m = 0: deactivated (not activated)
- h = 1: inactivated
- h = 0: deinactivated (released from inactivation)

Voltage-gated ionic channels:

- Activating gates: open the channels
- Inactivating gates: close the channels

 $I = G_X p (V - E_X)$ $p = m^a h^b$

- persistent currents: do not inactivate (b = 0)
- transient currents: do inactivate

Voltage-gated ionic channels: diagram

 $\begin{array}{c} \alpha(V) \\ \xleftarrow{} 0 \\ \beta(V) \end{array} O$

C: closed states

O: open states

 $\alpha(V)$: rate constant at which the gate goes from the closed to the open states

 $\beta(V)$: rate constant at which the gate goes from the open to the closed states

Voltage-gated ionic channels: diagram

 $\begin{array}{c} \alpha(V) \\ \longleftrightarrow \\ \beta(V) \end{array} O$

m: fraction of open gates

1-m: fraction of closed states

$$\frac{\mathrm{d}m}{\mathrm{d}t} = \alpha(V)(1-m) - \beta(V)m$$
$$\frac{\mathrm{d}m}{\mathrm{d}t} = (m_{\infty}(V) - m)/\tau(V)$$

$$m_{\infty}(V) = \frac{\alpha(V)}{\alpha(V) + \beta(V)} \qquad \qquad \tau(V) = \frac{1}{\alpha(V) + \beta(V)}$$

$$\begin{array}{rcl} C\,\dot{V} &=& I &-& \overbrace{\bar{g}_{\rm K} n^4 (V-E_{\rm K})}^{I_{\rm K}} &-& \overbrace{\bar{g}_{\rm Na} m^3 h (V-E_{\rm Na})}^{I_{\rm Na}} &-& \overbrace{\bar{g}_{\rm L} (V-E_{\rm L})}^{I_{\rm L}} \\ \dot{n} &=& \alpha_n (V) (1-n) - \beta_n (V) n \\ \dot{m} &=& \alpha_m (V) (1-m) - \beta_m (V) m \\ \dot{h} &=& \alpha_h (V) (1-h) - \beta_h (V) h \ , \end{array}$$

$$\alpha_n(V) = 0.01 \frac{10 - V}{\exp(\frac{10 - V}{10}) - 1} \qquad \alpha_m(V) = 0.1 \frac{25 - V}{\exp(\frac{25 - V}{10}) - 1} \qquad \alpha_h(V) = 0.07 \exp\left(\frac{-V}{20}\right)$$

$$\beta_n(V) = 0.125 \exp\left(\frac{-V}{80}\right) \qquad \beta_m(V) = 4 \exp\left(\frac{-V}{18}\right) \qquad \beta_h(V) = \frac{1}{\exp(\frac{30 - V}{10}) + 1}$$

$$\begin{array}{rcl} C\dot{V} &=& I &-& \overbrace{\bar{g}_{\rm K} n^4 (V-E_{\rm K})}^{I_{\rm K}} &-& \overbrace{\bar{g}_{\rm Na} m^3 h (V-E_{\rm Na})}^{I_{\rm Na}} &-& \overbrace{\bar{g}_{\rm L} (V-E_{\rm L})}^{I_{\rm L}} \\ \dot{n} &=& (n_{\infty}(V)-n)/\tau_n(V) \ , \\ \dot{m} &=& (m_{\infty}(V)-m)/\tau_m(V) \ , \\ \dot{h} &=& (h_{\infty}(V)-h)/\tau_h(V) \ , \end{array}$$

$$\begin{aligned} n_{\infty} &= \alpha_n / (\alpha_n + \beta_n) , & \tau_n &= 1 / (\alpha_n + \beta_n) , \\ m_{\infty} &= \alpha_m / (\alpha_m + \beta_m) , & \tau_m &= 1 / (\alpha_m + \beta_m) , \\ h_{\infty} &= \alpha_h / (\alpha_h + \beta_h) , & \tau_h &= 1 / (\alpha_h + \beta_h) \end{aligned}$$



Figure 2.13: Steady-state (in)activation functions (left) and voltage-dependent time constants (right) in the Hodgkin-Huxley model.

$$\begin{split} C\dot{V} &= I - \overbrace{\bar{g}_{\mathrm{K}} n^{4}(V - E_{\mathrm{K}})}^{I_{\mathrm{K}}} - \overbrace{\bar{g}_{\mathrm{Na}} m^{3}h(V - E_{\mathrm{Na}})}^{I_{\mathrm{Na}}} - \overbrace{g_{\mathrm{L}}(V - E_{\mathrm{L}})}^{I_{\mathrm{L}}} \\ \dot{n} &= \alpha_{n}(V)(1 - n) - \beta_{n}(V)n \\ \dot{m} &= \alpha_{m}(V)(1 - m) - \beta_{m}(V)m \\ \dot{h} &= \alpha_{h}(V)(1 - h) - \beta_{h}(V)h , \end{split}$$

$$E_{\rm K} = -12 \text{ mV}$$
 $E_{\rm Na} = 120 \text{ mV}$ $E_{\rm L} = 10.6 \text{ mV}$
 $\bar{g}_{\rm K} = 36 \text{ mS/cm}^2$ $\bar{g}_{\rm Na} = 120 \text{ mS/cm}^2$ $g_{\rm L} = 0.3 \text{ mS/cm}^2$











Figure 2.16: Positive and negative feedback loops resulting in excited (regenerative) behavior in neurons.