Introduction to Computational Neuroscience

Biol 698 Math 635 Biol 498 Math 430

Neuronal Networks

Reference:

• *Mathematical Foundations of Neuroscience*, by G. B. Ermentrout & D. H. Terman - Springer (2010), 1st edition. ISBN 978-0-387-87707-5

• Phase plane analysis of neural nets. B Ermentrout. InThe Handbook of Brain Theory and Neural Networks. MIT Press (2007)



Firing rate models - Single cells

Firing rate model - Population of neurons

Markov The Wilson-Cowan equations

Populations of excitatory neurons

Populations of inhibitory neurons

Up-down states

POPULATION MODELS

Firing rate models / population models:

Modgkin-Huxley-type models track the spiking of every neuron

Firing rate models track the averaged behavior of the spike rates of groups of neurons within the circuit

Rate models are the underlying "biology" in the theory of neural networks

Connectionist and back-propagation models are connected through rate models

 $\mathbf{v}_{i}(t)$: observable output

☑ V_i(t): somatic potential

 $\mathbf{v}_{i}(t)$ and $V_{i}(t)$ depend in a nonlinear way

 $u_i(t) = F_i(V_i(t))$

 $\boxed{\mathbf{M}}$ $\mathbf{u}_{i}(t)$ determines the instantaneous number of spikes that a neuron fires in an infinitesimal time interval

☑ u_i(t)dt: probability of a spike occurring in the time interval (t,t+dt)



Schematic of a pair of neurons synaptically coupled

 $\checkmark \Phi_{ij}$: postsynaptic potential appearing on postsynaptic cell i due to a single spike from presynaptic cell j

 \mathbf{v} t₁, t₂, ..., t_m: firing time of the presynaptic cell

 $\mathbf{O}G_{ij}(t)$: total potential received at the soma

$$G_{ij}(t) = \sum_{l} \Phi_{ij}(t - t_l)$$

 $\overbrace{\mathcal{I}}^{\tau_{ij}}$: axonal delay in the spike arising at cell **j** arriving at cell **i**



Schematic of a pair of neurons synaptically coupled

$$G_{ij}(t) = \int_{t_0}^t \Phi_{ij}(t-s)u_j(s-\tau_{ij})ds$$

Assumption: linear summation

$$u_{i}(t) = F_{i}(V_{i}(t)) \qquad \qquad G_{ij}(t) = \int_{t_{0}}^{t} \Phi_{ij}(t-s)u_{j}(s-\tau_{ij})ds$$

$$V_{i}(t) = \sum_{j} G_{ij}(t) = \sum_{j} \int_{t_{0}}^{t} \Phi_{ij}(t-s) F_{j}(V_{j}(s-\tau_{ij})) ds$$

$$u_i(t) = F_i\left(\sum_j \int_{t_0}^t \Phi_{ij}(t-s)u_j(s-\tau_{ij})ds\right)$$

 \mathbf{M} R_M: membrane resistance

 \mathbf{v}_{m} : time constant

I: presynaptic current

$$\tau_m \frac{\mathrm{d}\Phi}{\mathrm{d}t} + \Phi = R_\mathrm{M} I(t)$$

Assumption:

$$I(t) = \exp(-t/\tau_d) - \exp(-t/\tau_r)$$

 $\mathbf{v}_{\mathbf{r}}$: rise time

 \mathbf{V} τ_d : decay time

$$\Phi(t) = \frac{\tau_d}{\tau_d - \tau_m} \left(e^{-t/\tau_d} - e^{-t/\tau_m} \right) - \frac{\tau_r}{\tau_r - \tau_m} \left(e^{-t/\tau_r} - e^{-t/\tau_m} \right)$$

 \mathbf{M} If Φ is a sum of exponentials, the integral equation can be broken into a set of differential equations

$$x(t) = \int_{t_0}^t e^{-(t-s)/\tau} y(s-r) ds$$

$$\frac{\mathrm{d}x}{\mathrm{d}t} = y(t-r) - \frac{1}{\tau} \int_{t_0}^t \mathrm{e}^{-(t-s)/\tau} y(s-r) \mathrm{d}s = y(t-r) - x(t)/\tau.$$

$$\frac{\mathrm{d}x}{\mathrm{d}t} + x/\tau = y(t-r)$$

 \mathbf{M} Homogeneous populations of neurons: $\Phi_{ij} = w_{ij} \Phi$

W_{ij}: magnitude of the connections

$$V_{i}(t) = \sum_{j} G_{ij}(t) = \sum_{j} \int_{t_{0}}^{t} \Phi_{ij}(t-s) F_{j}(V_{j}(s-\tau_{ij})) ds$$

$$(LV_i)(t) = \sum_j w_{ij} F_j (V_j(t-r))$$

M L: linear homogeneous differential operator

 \mathbf{M} Homogeneous populations of neurons: $\Phi_{ij} = w_{ij} \Phi$

- \mathbf{v}_{ij} : magnitude of the connections
- \mathbf{V} \mathbf{z}_{ij} : synaptic drive

$$u_i(t) = F_i\left(\sum_j \int_{t_0}^t \Phi_{ij}(t-s)u_j(s-\tau_{ij})ds\right)$$

$$z_i(t) = \int_{t_0}^t \Phi(t-s)u_i(s-r)ds$$

$$(Lz_i)(t) = u_i(t-r) = F_i\left(\sum_j w_{ij}z_j(t-r)\right)$$

 \mathbf{V} Less restrictive assumption: $\Phi_{ij} = \mathbf{w}_{ij} \Phi_i$

W_{ij}: magnitude of the connections

Z_{ij}: synaptic drive

$$(L_i V_i)(t) = \sum_j w_{ij} F_j (V_j (t-r))$$

 \mathbf{V} Less restrictive assumption: $\Phi_{ij} = W_{ij} \Phi_j$

$$(L_i z_i)(t) = F_i\left(\sum_j w_{ij} z_j(t-r)\right)$$

What's the meaning of these assumptions?

 $\mathbf{M} \Phi_{ij} = \mathbf{w}_{ij} \Phi_i$: the response of neuron **i** to any inputs depends (up to a scalar constant which could be negative or positive) only on the properties of the postsynaptic cell

☑ Valid assumption if the shape and temporal properties of the presynaptic currents are the same no matter what type the presynaptic cell is (NMDA is slower than AMPA; AMPA is faster than GABA)

 $\boldsymbol{\boxed{\prime}} \tau_m \gg \{\tau_d, \tau_r\} \rightarrow \Phi(t) \approx \exp(-t/\tau_m)/\tau_m$

$$\tau_{m,i}\frac{\mathrm{d}V_i(t)}{\mathrm{d}t} + V_i(t) = \sum_j w_{ij}F_j(V_j(t-r))$$

What's the meaning of these assumptions?

 $\mathbf{v} \Phi_{ij} = w_{ij} \Phi_{j}$: the shape of the postsynaptic potential depends only on the presynaptic cell

We can distinguish different types of synapses (and it allows incorporation of synaptic depression and facilitation

 $\mathbf{v}_{d} \gg \{\tau_{m}, \tau_{r}\} \rightarrow \Phi_{j}(t) \approx \exp(-t/\tau_{d})/\tau_{d}$

$$\tau_d \frac{\mathrm{d}z_i(t)}{\mathrm{d}t} + z_i(t) = F_i\left(\sum_j w_{ij} z_j(t-r)\right)$$

Conductance-based network model

$$C\frac{\mathrm{d}V_i}{\mathrm{d}t} + I_i(V_i, \ldots) = -\sum_j g_{ij}s_j(V_i - V_{\mathrm{syn},j}),$$
$$\tau_{\mathrm{syn}}\frac{\mathrm{d}s_i}{\mathrm{d}t} + s_i = R_i(V_i, s_i).$$

 \mathbf{V} I_i: all nonlinear conductances which lead to action potentials

Solution: Assumption: a synapse from cell j produces the same conductance change regardless of the postsynaptic target

 \checkmark Assumption: $\tau_m \gg 1$ (slow synapses) $\rightarrow s_i = const$

 \checkmark Assumption: $V_{syn,j} = V_e$ (all neurons are excitatory)

Conductance-based network model

$$C\frac{\mathrm{d}V_i}{\mathrm{d}t} + I_i(V_i, \ldots) = -\sum_j g_{ij}s_j(V_i - V_{\mathrm{syn},j}),$$
$$\tau_{\mathrm{syn}}\frac{\mathrm{d}s_i}{\mathrm{d}t} + s_i = R_i(V_i, s_i).$$

$$G_i = \sum_j g_{ij} s_j$$

M Bifurcation diagram:

 $V_i(t) = \bar{V}_i(t; G_i)$

 \checkmark Two types of behavior: stable fixed-points and limit cycles with period $T_i(G_i)$

Conductance-based network model

$$C\frac{\mathrm{d}V_i}{\mathrm{d}t} + I_i(V_i, \ldots) = -\sum_j g_{ij}s_j(V_i - V_{\mathrm{syn},j}),$$
$$\tau_{\mathrm{syn}}\frac{\mathrm{d}s_i}{\mathrm{d}t} + s_i = R_i(V_i, s_i).$$

$$G_i = \sum_j g_{ij} s_j \qquad \qquad V_i(t) = \bar{V}_i(t; G_i)$$

$$\frac{\mathrm{d}s_i}{\mathrm{d}t} = \frac{1}{\tau_{\mathrm{syn}}}(-s_i + R_i(\bar{V}_i(t;G_i),s_i)).$$

Fixed-point case: straightforward

M Limit cycle case: averaging



$$\frac{\mathrm{d}s_i}{\mathrm{d}t} = \frac{1}{\tau_{\mathrm{syn}}} (-s_i + \langle R_i(\bar{V}_i(t;G_i), s_i) \rangle)$$

$$\langle R_i(\bar{V}_i(t;G_i),s_i)\rangle = \frac{1}{T_i(G_i)} \int_0^{T_i(G_i)} R_i(\bar{V}_i(t;G_i),s_i) dt \equiv Q_i(G_i,s_i)$$

$$\tau_{\rm syn}\frac{{\rm d}s_i}{{\rm d}t} + s_i = Q_i\left(\sum_j g_{ij}s_j, s_i\right)$$



$$\frac{\mathrm{d}s}{\mathrm{d}t} = \alpha(V)(1-s) - \beta s$$

$$\beta = 1/\tau_{\rm syn}, \qquad \qquad R(V,s) = \alpha(V)\tau_{\rm syn}(1-s)$$

 \mathbf{M} $\alpha(V)$ is zero except when the neuron spikes

☑ Assumption: the width of a spike is independent of the firing rage of the neuron

$$\mathbf{V}$$
 Q(G,s):

$$\int_0^T \alpha(\bar{V}(t))\tau_{\rm syn} \mathrm{d}t = \mu$$

 $\mathbf{\underline{M}}\mu$ is a constant independent of T

F(**G**): firing rate of the conductance-based model given the synaptic conductance **G**

$$F(G) \equiv \frac{1}{T(G)}$$

$$Q_i(G_i, s_i) \equiv \frac{1}{T_i(G_i)} \int_0^{T_i(G_i)} R_i(\bar{V}_i(t; G_i), s_i) dt = \mu_i F_i(G_i)(1 - s_i)$$

$$\tau_{\rm syn}\frac{{\rm d}s_i}{{\rm d}t}+s_i=Q_i\left(\sum_j g_{ij}s_j,s_i\right)$$

$$Q_i(G_i, s_i) \equiv \frac{1}{T_i(G_i)} \int_0^{T_i(G_i)} R_i(\bar{V}_i(t; G_i), s_i) dt = \mu_i F_i(G_i)(1 - s_i)$$

$$\tau_i \frac{\mathrm{d}s_i}{\mathrm{d}t} = \mu_i F_i \left(\sum_j g_{ij} s_j\right) (1 - s_i) - s_i$$

POPULATION OF NEURONS

M The main role of firing rate models is to examine large numbers of neurons in some "average" fashion

Spiking events are probabilistic
Post-stimulus time histogram (PSTH): repetition of the same stimulus over many trials
PSTH is effectively a firing rate (number of spikes per unit of time)
PSTH assumes that recording simultaneously from N nearby locations and from one location N times give the same result
Assumption: neurons fire independently of each other
Then, the firing rate of the population and a single neuron are exactly the same: Population firing rate.

Is the independence assumption reasonable?

$$\tau_e \frac{\mathrm{d}E}{\mathrm{d}t} = -E + (1 - r_e E) F_e(\alpha_{ee} E - \alpha_{ie} I + T_e(t)),$$

$$\tau_i \frac{\mathrm{d}I}{\mathrm{d}t} = -I + (1 - r_i I) F_i(\alpha_{ei} E - \alpha_{ii} I + T_i(t)),$$

 \mathbf{M} T_e, T_i: input from the thalamus

 \mathbf{V} \mathbf{r}_{e} , \mathbf{r}_{i} : refractory fraction of the neurons available to fire

 \mathcal{M} (1-r_e E), (1 - r_i I): fraction of neurons available to fire given they have an absolute refractory period of r_e and r_i respectively

F(u): gain functions

$$F(u) = 1/(1 + \exp(-\beta(u - u_T)))$$

F(u): probability of firing (rather than an actual firing rate)

Scalar recurrent model:

$$\frac{\mathrm{d}u}{\mathrm{d}t} = -u + F(\alpha u + \beta)$$



 $\mathbf{\underline{M}} \beta$: input

Scalar recurrent model:

$$\frac{\mathrm{d}u}{\mathrm{d}t} = -u + F(\alpha u + \beta)$$

Fixed-point:

$$-u + F(\alpha u + \beta) = 0$$

 \mathbf{V} Control parameter: β

Saddle-node bifurcation:

 $-1 + \alpha F'(\alpha u + \beta) = 0$

M Two-population networks

$$\tau_1 u_1' = -u_1 + F_1(w_{11}u_1 + w_{12}u_2),$$

$$\tau_2 u_2' = -u_2 + F_2(w_{21}u_1 + w_{22}u_2).$$

Theorem. Consider the planar system

$$\begin{aligned} x' &= f(x, y), \\ y' &= g(x, y), \end{aligned}$$

such that $f_y g_x > 0$ for all (x, y). Then there are no limit cycles.

If $F'_i(u) > 0$ and $w_{12}w_{21} > 0$, then there are no limit cycles and there are just fixed points

$$\tau_1 x_1' = -x_1 + f(w_{11}x_1 + w_{12}x_2 + s_1)$$

$$\tau_2 x_2' = -x_2 + f(w_{21}x_1 + w_{22}x_2 + s_2)$$

⊠ x₁-nullcline

$$x_2 = (-w_{11}x_1 - s_1 + f^{-1}(x_1))/w_{12}$$

 \mathbf{V} x₂-nullcline

$$x_1 = (-w_{22}x_2 - s_2 + f^{-1}(x_2))/w_{21}$$

 $M(x) = (-w_s x - s f^{-1}(x))/w_c$

 $f(x) = 1 / (1 + \exp(-x))$

h(x) is monotone if
 w_s is positive
 small and negative

h is cubic
 w_s is large
 wc determines the properties of h



M Two-population networks

 $\tau_1 u'_1 = -u_1 + F_1(w_{11}u_1 + w_{12}u_2),$ $\tau_2 u'_2 = -u_2 + F_2(w_{21}u_1 + w_{22}u_2).$



Fig. 11.2 Nullcline configurations for mutually excitatory-inhibitory networks: (a) mutual excitation, (b) mutual inhibition, (c) mutual excitation with weak self-connections

Any fixed-points which occur on the intersection of two outer branches: stable node
 Any fixed-points which occur on the intersection of two inner branches: unstable node
 Any other fixed-point: saddle

Choice between two or more competing sensory inputs



Competition between two neural pools or populations

 $\tau_1 u'_1 = -u_1 + F_1(w_{11}u_1 + w_{12}u_2),$ $\tau_2 u'_2 = -u_2 + F_2(w_{21}u_1 + w_{22}u_2).$



$$F(u) = 1/(1 + \exp(-(u - 1)))$$
 $w = 5$

Competition between two neural pools or populations

Solution of the same (low) value fire equally at the same (low) value

Intermediate input values:

Homogeneous fixed-point is unstable

Two stable fixed-points: "winning" units

Separatrix (blue arrows): stable manifold of the saddle.

If High input values: both units fire equally at the same (high) value



Competition between two neural pools or populations

If there is a slight bias in the inputs, then as the input increases, the favored population will always win

With a strong enough perturbation it is possible to switch to the less favored population (for a limited range of inputs)

Isola:

small island of solutions
 fold bifurcations (arrows)
 As the bias disappears, the isola grows and merges with the main branch of solutions
 As the bias increases, the isola shrinks to a point and disappears
 Symmetry-breaking instabilities, bifurcations and pattern formation: the symmetric solution loses stability owing to the negative interactions and results in new solutions which are no longer symmetric



Excitatory-inhibitory pairs

$$\tau_1 u_1' = -u_1 + F(w_{11}u_1 - w_{12}u_2 + I_1),$$

$$\tau_2 u_2' = -u_2 + F(w_{21}u_1 - w_{22}u_2 + I_2).$$





Fig. 11.4 Sample bifurcation diagram for an excitatory and inhibitory population. The parameters are $w_{11} = 12$, $w_{12} = 10$, $w_{21} = 16$, $w_{22} = 4$, and $\tau = 2$. (a) Behavior of u_1 as I_1 increases, $I_2 = -4$. (b) Two-parameter diagram as a function of the inputs, I_1 , I_2 . Green circles indicate Takens-Bogdanov points. (c) Phase plane for $I_2 = -4$, $I_1 = 0$

Up-down states

☑ In prefrontal cortical slices, local recurrent networks of excitatory and inhibitory neurons are able to produce epochs of sustained firing both spontaneously and through stimulation

MTwo states: firing and quiescent

Observed in extracellular and intracellular recordings of neurons

Up-down states



Fig. 11.5 Modeling up and down states in cortex. (a) Experimental data from Shu et al. [247] showing (a) extracellular (*upper curve*) and intracellular (*lower curve*) recordings over about 10 s, and (b) evoked states via external stimuli. (b) Simulation of up-down states in a noisy Wilson-Cowan model showing spontaneous switching. (c) Phase-plane explanation of the balanced bistable state. The parameters are $\tau_1 = 5$, $\tau_2 = 3$, $w_{11} = 16$, $w_{21} = 24$, $w_{12} = 10$, $w_{22} = 6$, $I_1 = -3.7$, and $I_2 = -6.7$. Colored noise is added to the inputs. *SM* stable manifold

Up-down states

M The network undergoes bouts of sustained activity lasting up to 4s followed by quiescence

☑ During bouts of activity, the membrane potential is depolarized (``up state") compared with that during the quiescent period (``down state")

Stimuli allow one to switch from the down to the up state and vice-versa

O Depolarizing stimuli can switch the network from the up to the down state (!)

When the network is in the down state, very strong stimuli cause a brief bout of activity immediately followed by a return to the down state.



Up-down states



Fig. 11.5 Modeling up and down states in cortex. (a) Experimental data from Shu et al. [247] showing (a) extracellular (*upper curve*) and intracellular (*lower curve*) recordings over about 10 s, and (b) evoked states via external stimuli. (b) Simulation of up-down states in a noisy Wilson-Cowan model showing spontaneous switching. (c) Phase-plane explanation of the balanced bistable state. The parameters are $\tau_1 = 5$, $\tau_2 = 3$, $w_{11} = 16$, $w_{21} = 24$, $w_{12} = 10$, $w_{22} = 6$, $I_1 = -3.7$, and $I_2 = -6.7$. Colored noise is added to the inputs. *SM* stable manifold

Up-down states - phase plane

Two stable fixed-points: up and down states (bistable system)

Saddle point separating these states. Its stable manifold acts as a threshold

Modest stimuli will take the system from the down to the up state and vice-versa

If a stimulus takes the excitatory population beyond about 0.4, then there will be an immediate return to the down state

Curved stable manifold allows switches from up to down due to strong depolarization

A depolarizing shock in the up state can take the system to the down state



Up-down states - phase plane

Delay before going on the down state which is dependent on the amplitude of the stimulus (stimulus close to the stable manifold but slightly beyond the right-hand branch will take much longer to go the the down state than will a stronger stimulus)

Strong stimuli during the down state can induce a brief period of activation followed by a return to the down state as well

Adding small amounts of noise to the model equations can cause spontaneous transitions between up and down states

Upper state is closer to instability and hass complex eigenvalues. This could explain the fact that the upper state is much noisier than the lower state







